

(4) 応用

逆問題とは？

- 順問題:

原因 結果

- 逆問題:

原因 結果

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(i) 電子顕微鏡の画像再構成

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実問題に対する応用 1/3

提案法の有効性を実問題で評価するために
電子顕微鏡の画像再構成問題に適用した

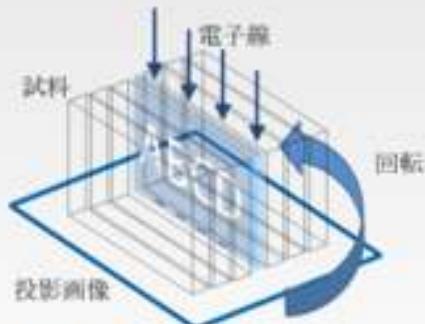


Figure: 電子顕微鏡の画像再構成問題.

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Inverse problems: Image reconstruction

In order to evaluate the proposed methods in practice, we apply them to image reconstruction problems

Consider approximating a solution x^* of linear systems of equations

$$Ax^* = b^*,$$

where $A \in \mathbb{R}^{m \times n}$ is a discretized Radon transform, $m \leq n$, $x^* \geq 0$ is an image data, and b^* is a projection data.

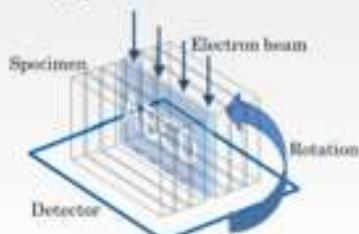


Figure: Projection image.

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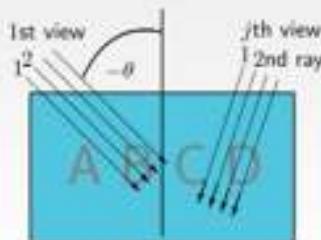
Difficulties 1/2

For simplicity, consider one slice of a specimen, i.e., 2D reconstruction.

Artifacts

Since the range of the angle θ of rotation of the specimen is limited due to physical constraints, reconstructed images may suffer artifacts. For instance,

$$-70^\circ < \theta < 70^\circ.$$



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Difficulties 2/2

Observation error

Since an observation error δ perturbs b^* , we actually treat

$$Ax = b \quad \text{or} \quad \min_{x \in \mathbb{R}^n} \|b - Ax\|_2.$$

to obtain $x \approx x^*$, where $b = b^* + \delta$.

Hence, a tight fitting $\min_{x \in \mathbb{R}^n} \|b - Ax\|_2$ gives an error-contaminated solution.



Figure: Exact image



Figure: Reconstructed image given by ART without observation error

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Previous methods 1/5

Algebraic Reconstruction Technique [Herman et al. '73]

- ART \iff the SOR method for the normal equations

$$AA^T \mathbf{u} = \mathbf{b}, \quad \mathbf{x} = A^T \mathbf{u}.$$

- Given $\mathbf{x}^{(0,1)}$, for $k = 0, 1, \dots$,

$$\begin{aligned}\mathbf{x}^{(k,i+1)} &= \mathbf{x}^{(k,i)} + \omega \frac{b_i - (\alpha_i, \mathbf{x}^{(k,i)})}{\|\alpha_i\|_2^2} \alpha_i, \quad i = 1, \dots, m, \\ \mathbf{x}^{(k+1,1)} &= \mathbf{x}^{(k,m+1)},\end{aligned}$$

where $\omega \in (0, 2)$ is the relaxation parameter and α_i is the i th row of A .

- If $\mathbf{x}^{(0,1)} = \mathbf{0}$, then ART gives the minimum-norm (pseudo-inverse) solution $\forall \mathbf{b} \in \mathcal{R}(A)$.

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Previous methods 2/5

Simultaneous Iterative Reconstruction Technique (SIRT) [Gilbert '72]

- SIRT \iff Richardson method for $A^T A \mathbf{x} = A^T \mathbf{b}$.

- Given $\mathbf{x}^{(0,1)}$, for $k = 0, 1, \dots$,

$$\mathbf{x}^{(k)} = \mathbf{x}^{(k-1)} + \omega A^T (\mathbf{b} - A \mathbf{x}^{(k-1)}),$$

where $\omega \in (0, 2/\|A^T A\|_2)$ is the relaxation parameter.

- SIRT gives the pseudo-inverse solution $\forall \mathbf{b} \in \mathbf{R}^m$.

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実問題に対する応用 2/3

提案法の有効性を数値実験で検討した



Figure: 再構成したい画像。



Figure: 従来法。相対誤差 0.621, 計算時間 180 秒。



Figure: 提案法。相対誤差 0.496, 計算時間 472 秒。
(相対誤差 0.617 のときは 72 秒。)

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実問題に対する応用 3/3

実際の観測データを用いた解法の性能比較



Figure: 従来法 A による再構成画像。



Figure: 従来法 B による再構成画像。



Figure: 提案法による再構成画像。

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Doctoral thesis, Department of Informatics, School of Multidisciplinary Sciences,
The Graduate University for Advanced Studies, June 10, 2013.

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(ii) 薬物動態モデルの逆問題

Cluster Newton Method

An Algorithm for Solving Underdetermined Inverse Problems: An Application to a Pharmacokinetics Model



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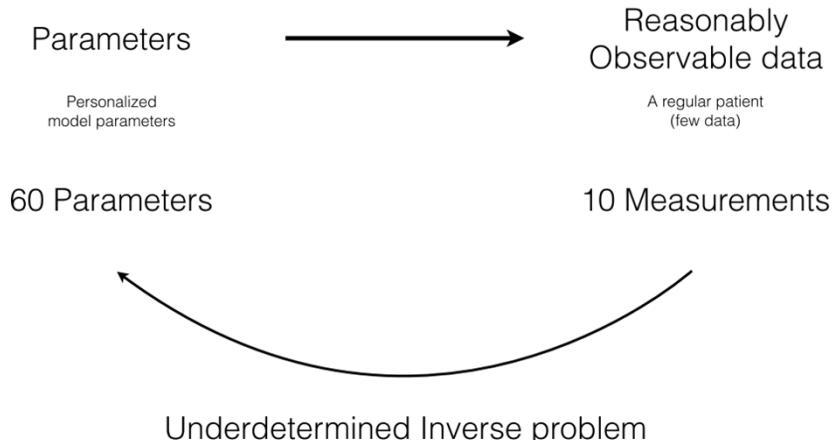
Akihiko Kanagaya
Tokyo Institute of Technology

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Personalized Pharmacokinetics Model of CPT-11

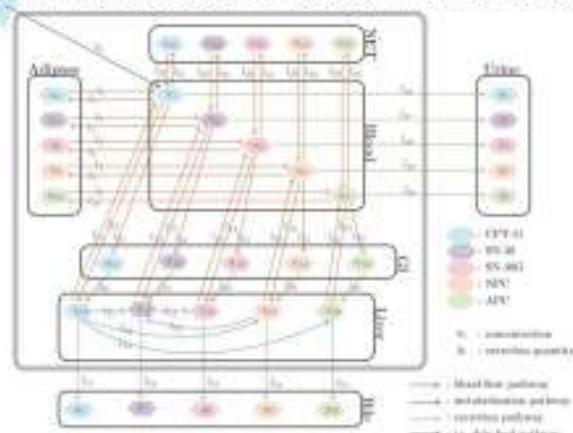


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Arikuma et al's Irinotecan PBPK model



$$\frac{d}{dt} u_{18} = \left(x_{12} \cdot a_3(t) + \frac{x_{23}}{x_9} \cdot a_{13}(t) + \frac{x_{45} \cdot x_{36} \cdot x_{37} \cdot x_{32} + x_{32} \cdot u_{18}(t)}{x_{13} \cdot x_{17} \cdot x_{23}} - \frac{x_{32} \cdot x_{23}}{x_{13}} \cdot u_{18}(t) \right) / x_{27}.$$

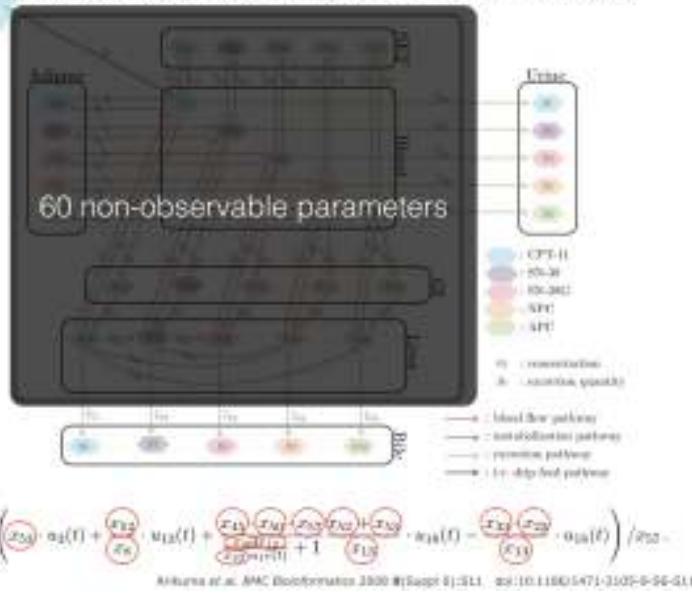
Arikuma et al. 2007C Biopharmaceutics 2008 • [Suppl 6] 50(1) – 60 | DOI:10.1111/j.1471-2203.2006.00641.x

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Arikuma et al's Irinotecan PBPK model

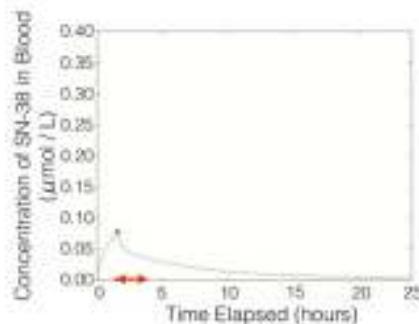


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This underdetermined inverse problem can easily be solved by the Levenberg-Marquardt method which finds a solution close to the initial model parameters.



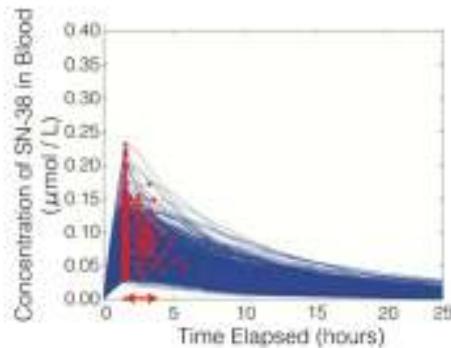
However, the clinical observation suggests that the maximum concentration should happen 2.5 ± 1 hour.

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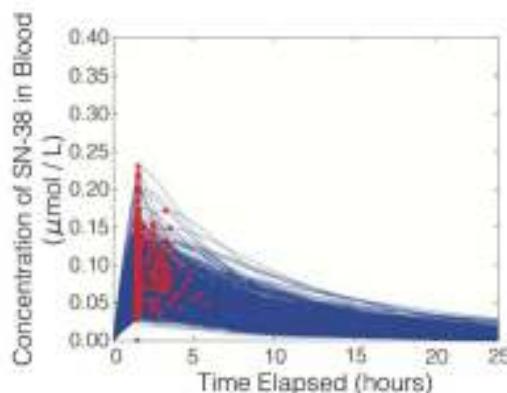
By solving this underdetermined inverse problem multiple times with different initial model parameters, we obtain various solutions which fits clinical observation.



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7~8 hours on a server machine with
two quad-core 3GHz Intel Xeon

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Why is this so time consuming?

- Function evaluation requires numerical solution of the system of non-linear ODEs.
- Jacobian is approximated by finite differences at each iteration for each solution.
- ODEs need to be solved fairly accurately in order for the LM method to converge to the root.

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Example 1 : Level curve tracing of a rough surface

Find a set of 100 points near \mathcal{X}^0 , s.t.

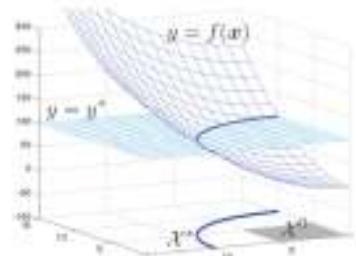
$$f(\mathbf{x}) = y^*$$

where

$$\begin{aligned} f(\mathbf{x}) &= (x_1^2 + x_2^2) \\ &+ \sin(10000x_1) \sin(10000x_2)/100 \end{aligned}$$

$$y^* = 100$$

$$\mathcal{X}^0 = \{\mathbf{x} \in \mathbb{R}^2 : \max_{i=1,2} \left| \frac{x_i - 2.5}{2.5} \right| < 1\}$$



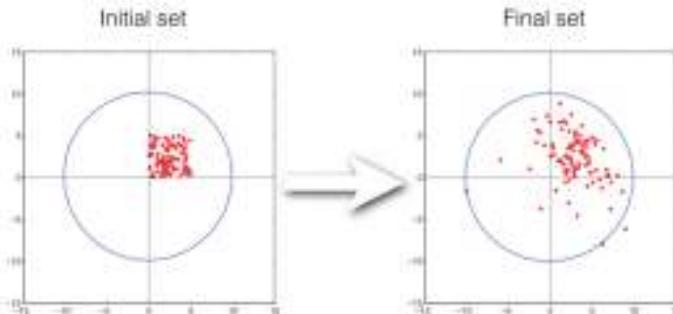
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Levenberg Marquardt method

For all of the initial points, the algorithm terminated with an error
 "Algorithm appears to be converging to a point that is not a root."



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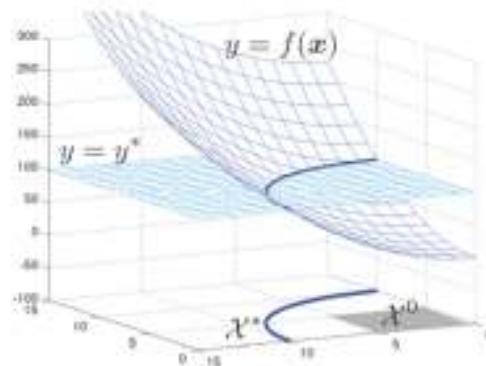
Cluster Newton method

- Stage 1 (Regularized Newton's method applied to a cluster of points)
 - Linear approximation with least squares fitting
 (least square solution of an overdetermined system of linear equations which acts as regularization)
 - Moore-Penrose inverse using the linear approximation
 (minimum norm solution of an underdetermined system of linear equations)
- Stage 2 (Broyden's method, i.e. multi-dimensional secant method)
 - Use the linear approximation in Stage 1 as initial Jacobian
 (start with reasonable Jacobian approximation)
 - Use the points found by the Stage 1 as initial points
 (start with the initial points already close to the solution)

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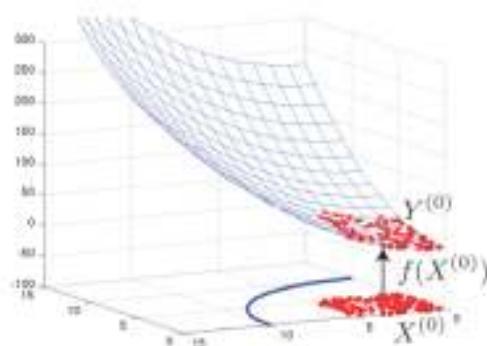
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Stage 1

1st iteration step1

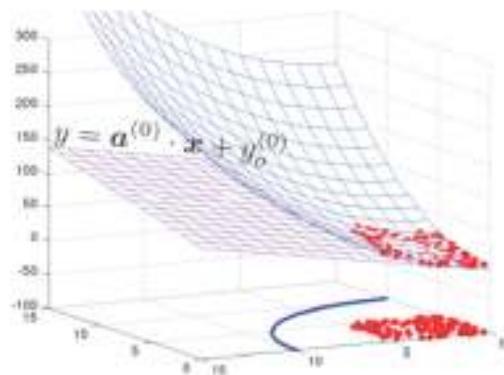


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Stage 1
1st iteration step2

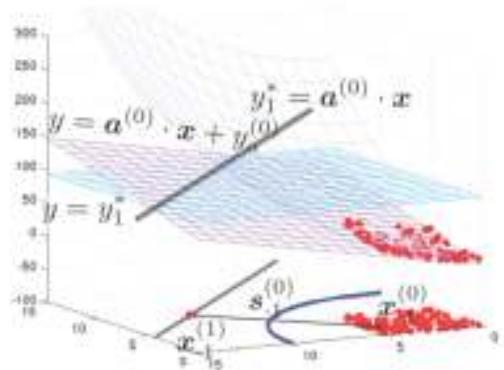


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Stage 1
1st iteration step3

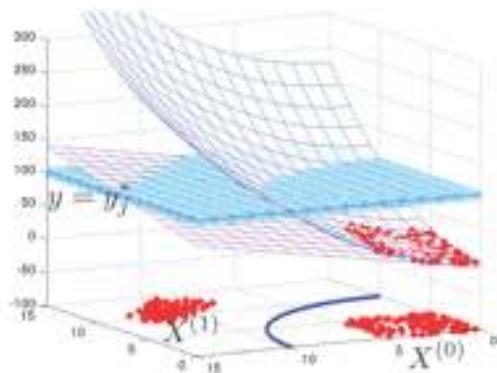


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Stage 1
1st iteration step4

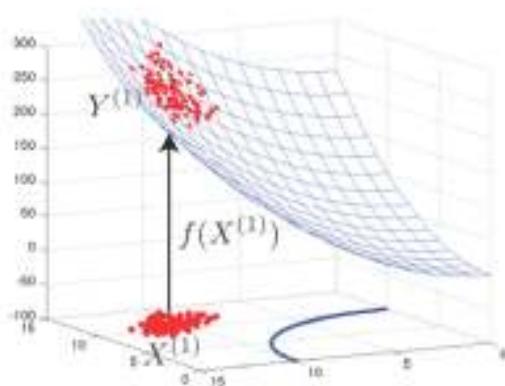


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Stage 1
2nd iteration step1

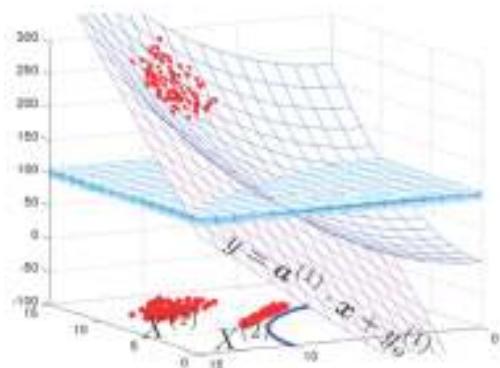


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Stage 1
2nd iteration step2-3

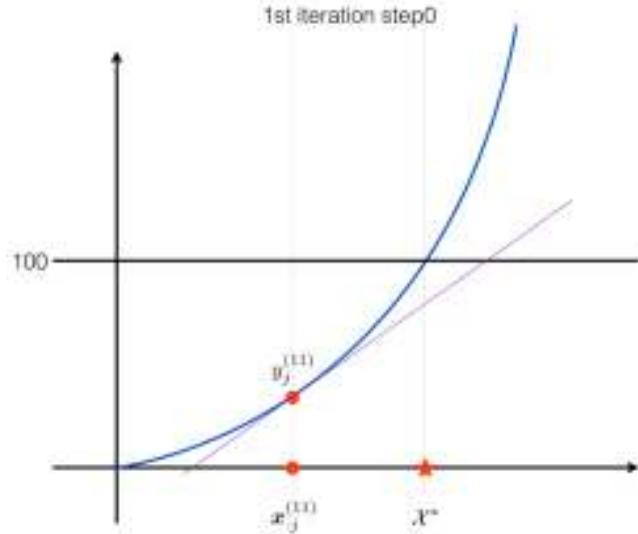


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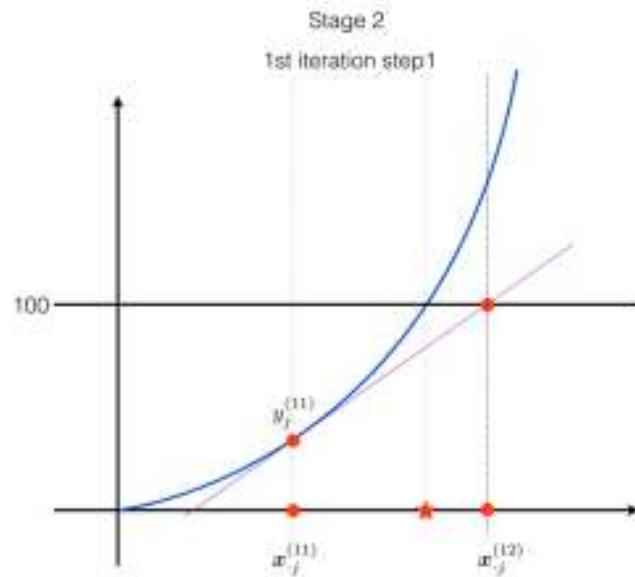
Stage 2
1st iteration step0



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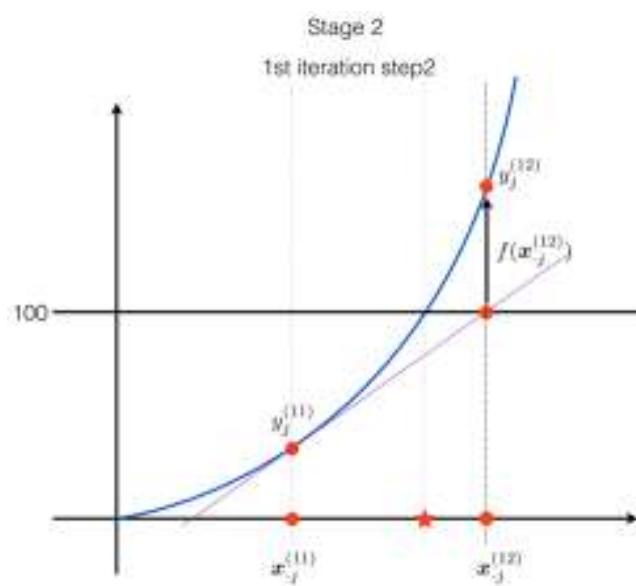
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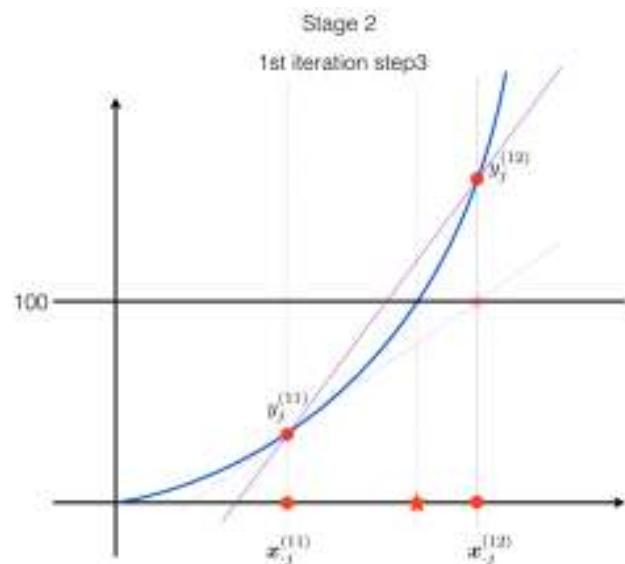
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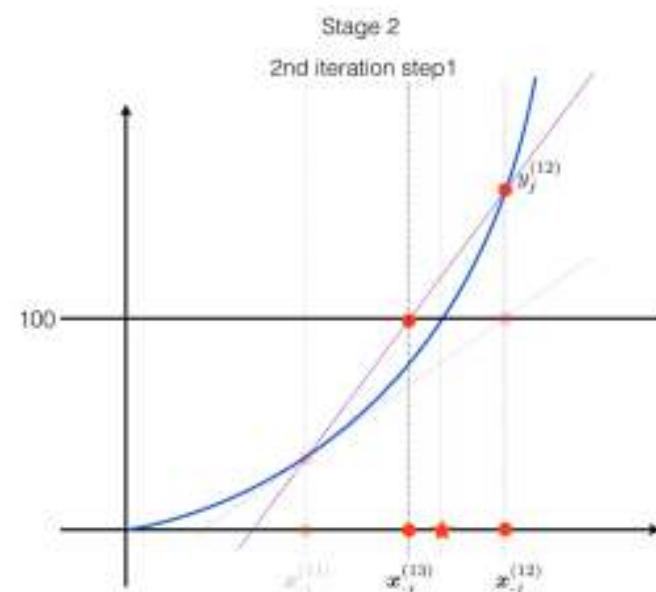
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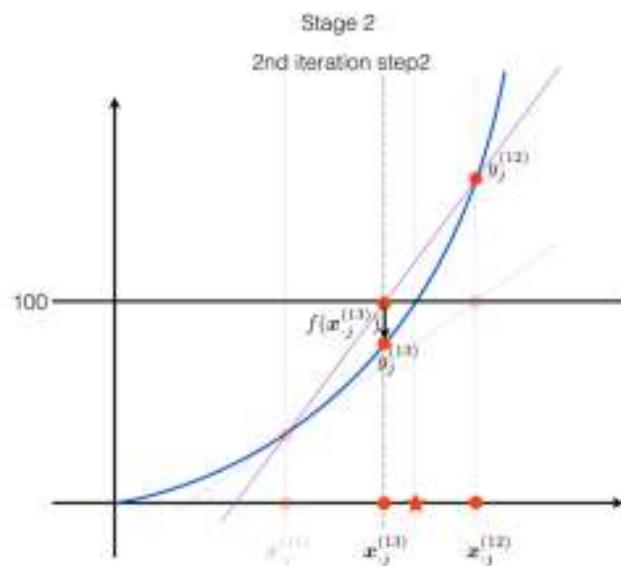
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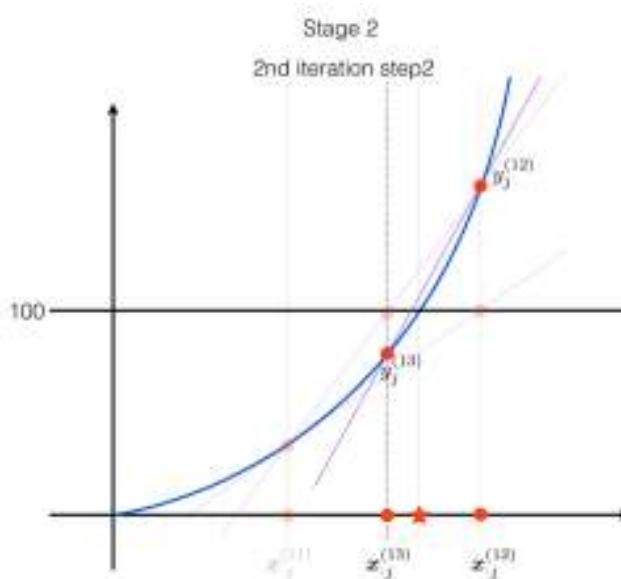
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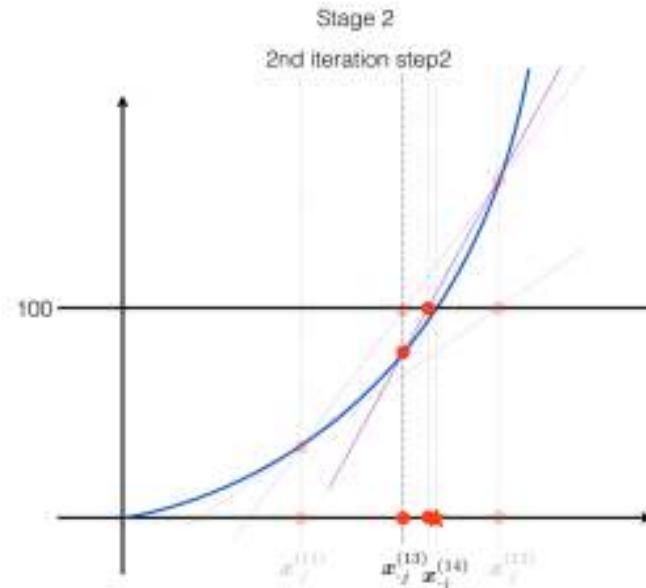
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Cluster Newton Method

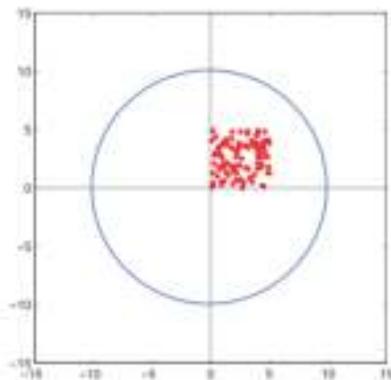
- 1 function evaluation / iteration / solution
- No Jacobian approximation based on the local info

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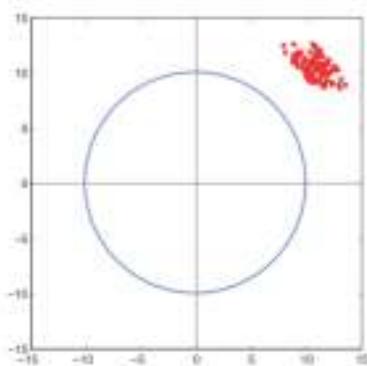
Initial set



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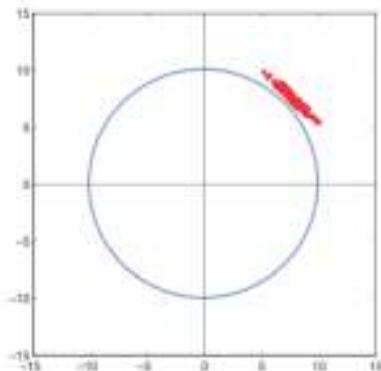
Stage 1
1st iteration

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Stage 1
2nd iteration

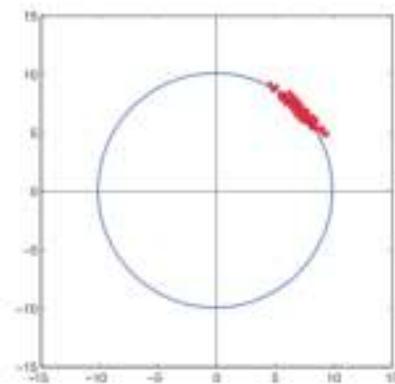


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Stage 1
3rd iteration

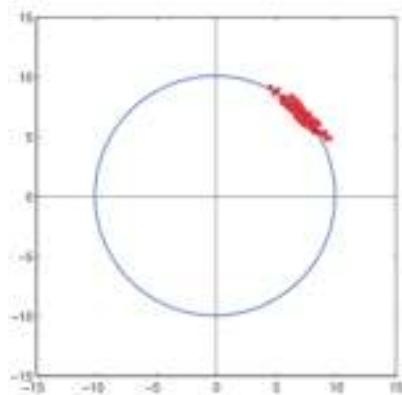


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Stage 1
4th iteration

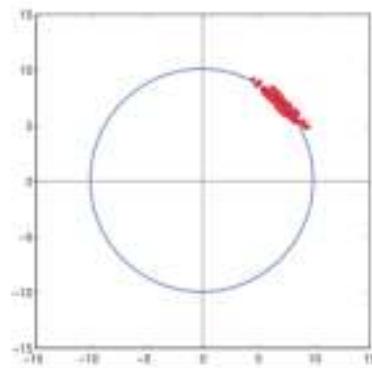


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Stage 1
5th iteration

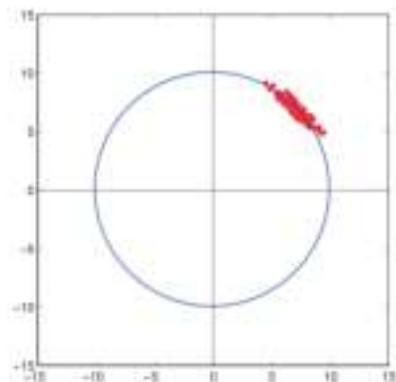


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Stage 1
6th iteration

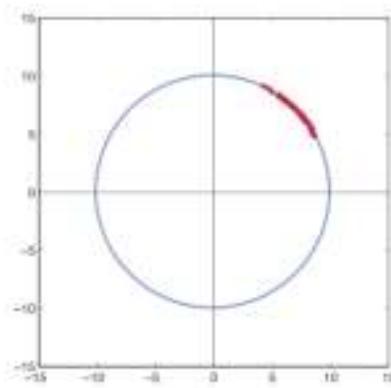


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Stage 2
1st iteration

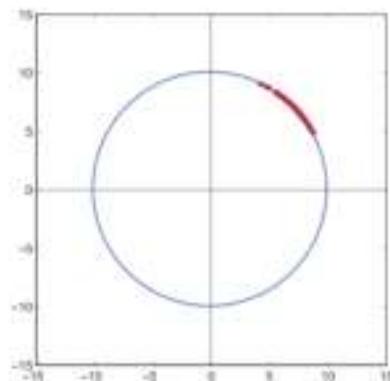


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Stage 2
2nd iteration

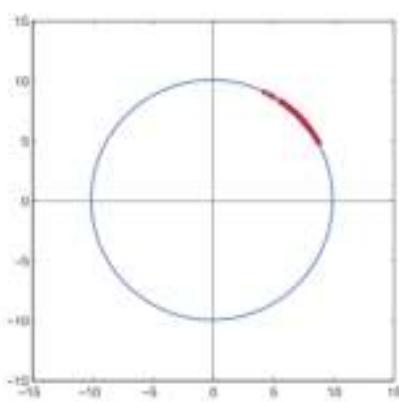


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Stage 2
3rd iteration

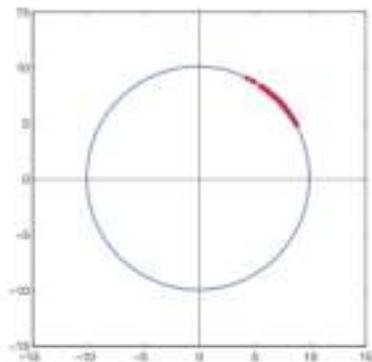


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Stage 2
4th iteration

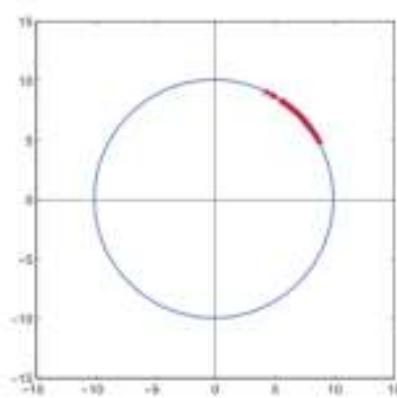


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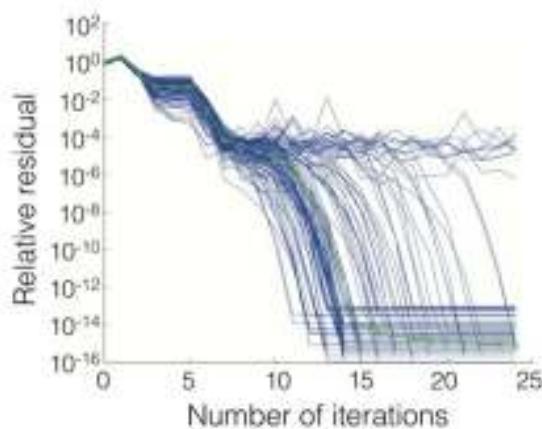
Stage 2
5th iteration



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$$\text{Relative residual : } r_j^{(k)} = \frac{|y_j^{(k)} - y^*|}{y^*}$$

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Example 2 : ODE coefficients identification

Forward Problem

Pharmacokinetics model of CPT-11 (Arikuma et al. 2008):

$$\frac{d}{dt} u = h(u, t; x)$$

where:

$u_{1,2,\dots,25}(t; x)$: concentration of drug/metabolites

$u_{26,\dots,35}(t; x)$: cumulative excretion quantity of drug/metab.

t : time

x : set of model parameters ($x \in \mathbb{R}^{60}$)

Map from model parameters to observable data:

$$f(x) = y$$

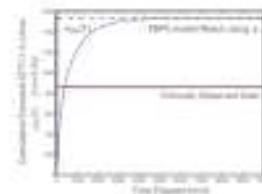
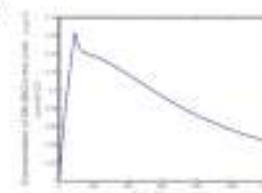
where y is a part of the steady state solution of the ODE

$$y_i(x) = \lim_{t \rightarrow \infty} u_{i+25}(t; x) \quad \text{for } i = 1, 2, \dots, 10$$

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Inverse Problem

Find 1000 sets of parameters \mathbf{x} , s.t.

$$\mathbf{f}(\mathbf{x}) = \mathbf{y}^*$$

where:

$$\mathbf{f} : \mathbb{R}^{60} \rightarrow \mathbb{R}^{10}$$

\mathbf{y}^* : clinically observed data

(Slatter et al. 2000)

| | clinically observed data | |
|----------------------------|--------------------------|-----------|
| | patient 1 | patient 2 |
| DPT-1T in Urine | y ₁ | 659.0 |
| DN-3G in Urine | y ₂ | 35.5 |
| SN-38G in Urine | y ₃ | 479.8 |
| MPC in Urine | y ₄ | 3.95 |
| APC in Urine | y ₅ | 305.0 |
| DPT-1G in Bladder + Faeces | y ₆ | 975.4 |
| DN-3G in Bladder + Faeces | y ₇ | 127.1 |
| SN-38G in Bladder + Faeces | y ₈ | 105.4 |
| MPC in Bladder + Faeces | y ₉ | 24.5 |
| APC in Bladder + Faeces | y ₁₀ | 219.4 |
| Mean Residual | $\sum_{i=1}^{10} y_i^2$ | 28461 |

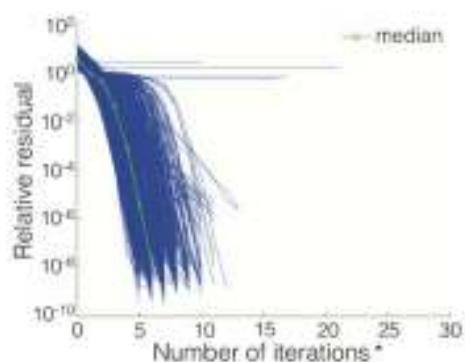
J. B. Slatter, L.-J. Sallaberry, P. R. Martin & A. P. Vennerstrom: D-Glutamyl Transpeptidase in Renal Tumours. J. Urol. 163, 103-106 (2000).
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Levenberg Marquardt method



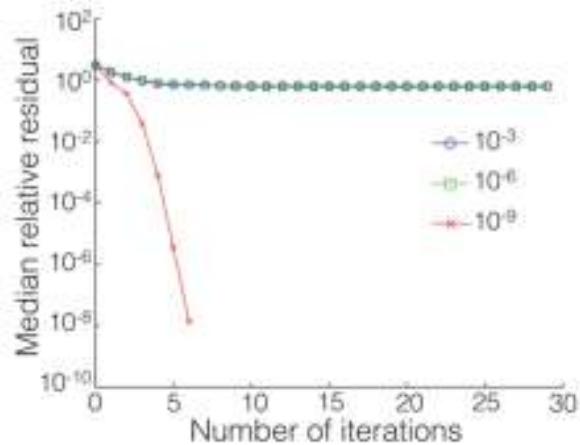
* : at least 61 function evaluations / iteration / solution

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Levenberg Marquardt method

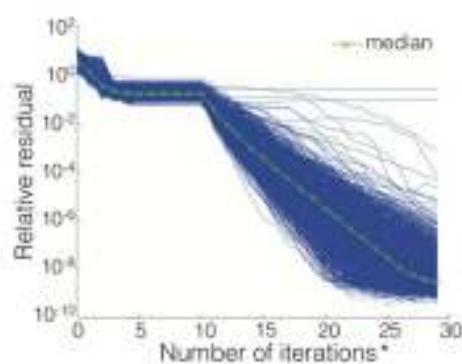


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Cluster Newton method



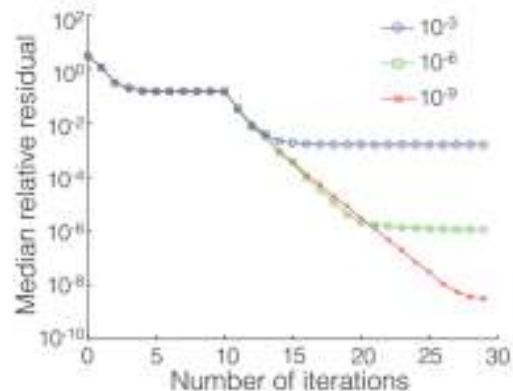
*: only 1 function evaluations / iteration / solution

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Cluster Newton method



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Cluster Newton method

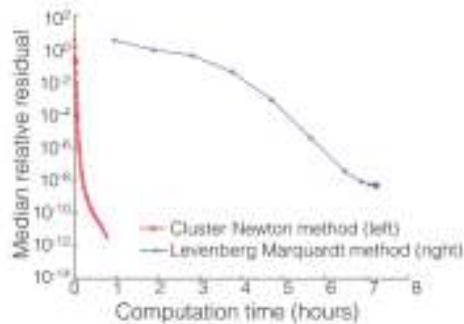
- Less number of function evaluations
- Less sensitive to the error in function evaluations

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Levenberg Marquardt method v.s. Cluster Newton method

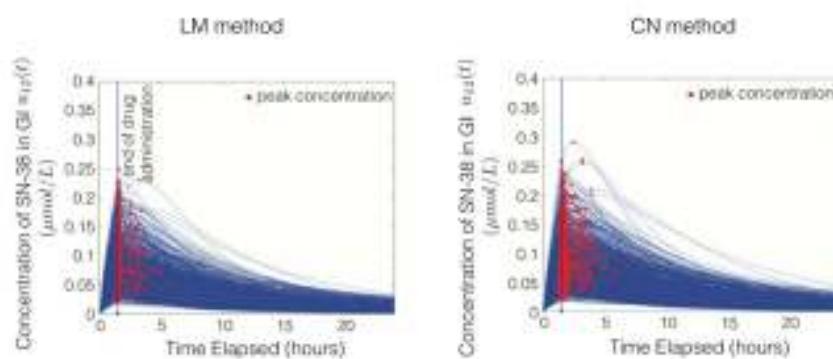


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Predicting un-measurable quantity through a mathematical model (concentration of SN-38 in gastrointestinal tract)



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Conclusion

We have introduced ...

- Idea of sampling multiple solutions in the solution manifold of an underdetermined inverse problem
- CN method efficiently finds multiple solutions.

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Reference

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